

Dissociated behavior of low-frequency responses and high-frequency oscillations after systemic morphine administration in conscious rats

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It has been proposed that high-frequency oscillations (HFOs) and underlying conventional somatosensory-evoked potentials (SEPs) have different brain origins. To further explore the neural mechanism of HFOs, we recorded the SEPs responding to high-intensity electrical stimulation applied to the hind paw of conscious, freely moving rats. We also investigated the effect of systemic morphine on HFOs and the conventional SEPs. HFOs after high-intensity electrical stimulation showed a widespread distribution in frontal and temporal regions of the brain. The amplitude of HFOs was significantly decreased by systemic morphine, whereas the primary conventional SEP components remained unaffected. The different changes in HFOs and primary SEP components after systemic morphine administration provided further evidence for the hypothesis that HFOs and underlying

conventional SEP components have different origins. *NeuroReport* 21:2–7 © 2010 Wolters Kluwer Health | Lippincott Williams & Wilkins.

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Introduction

High-frequency oscillatory activities (> 300 Hz) recorded in both humans and animals are drawing increasing attention on account of their unique features and possible functional roles. However, neural mechanisms underlying high-frequency oscillations (HFOs) remain unclear. Studies on somatosensory-evoked potentials (SEPs) and magnetoencephalography have revealed that HFOs are superimposed on the primary cortical response and can be extracted by digitally filtering the wide-band SEPs (10–2000 Hz) using a bandpass of 300–900 Hz [1–4]. Previous studies showed that the primary cortical response, N20, was most likely generated by excitatory postsynaptic potentials of pyramidal cells in area 3b [5]. On account of the specific relationship between the primary cortical responses and HFOs, it had been proposed that they have the same source. Subsequent studies, however, suggested that HFO was an independent SEP component dissociated functionally from the primary cortical response, because it either disappeared or became significantly smaller in amplitude during sleep, whereas the N20 remained almost constant [6–8]. Evidences from studies on the behavior of N20 and high-frequency wavelets under varying stimulus rates [9], different stimulus intensities [10], as well as lorazepam treatment [11] also support the hypothesis that they have different origins.

Pharmacological manipulation is a useful approach to study the possible neural mechanism of biological signals.

Morphine is a widely used analgesic that exerts its principal pharmacological effects on the central nervous system and produces significant effects of analgesia and sedation. Previous studies have shown that systemic morphine (5 mg/kg) preferentially attenuates the second pain mediated by unmyelinated C-fibers, whereas the first pain sensation mediated by myelinated A δ nociceptive afferents is relatively insensitive [12]. Therefore, morphine should have no effect on the primary SEP components, which reflect the conduction of nerve impulses to primary sensory centers. However, it is not clear how morphine affects the high-frequency SEP components. To examine the effect of morphine on HFOs and explore the underlying neural mechanisms, we recorded the SEPs after applying high-intensity electrical stimulation to the hind paw of conscious, freely moving rats before and after morphine administration.

Materials and methods

Animals and surgery

Adult male Sprague–Dawley rats weighing 300–350 g ($n=12$) were used in this experiment. All experiments were carried out in accordance with the Institutional Animal Care and Use Committee of Peking University Health Science Center.

Rats were anesthetized with ketamine (100 mg/kg, intraperitoneal) and fixed in a Kopf stereotaxic instrument. Twelve epidural electrodes (wired stainless-steel screws, tip diameter 1 mm, impedance 300–350 Ω) were

implanted symmetrically after the exposure of the skull. These recording electrodes were arranged 3 mm apart from anterior to posterior. Another two electrodes were positioned 2 and 4 mm caudal to the lambda at the midline as the reference and ground electrodes, respectively [13]. All the screws should be attached to the dura. The location of these electrodes is shown in the inset of Fig. 1. These electrodes were connected to a two-dimensional array connector and fixed to the skull with dental cement. Animals were then injected with antibiotics (penicillin, 60 000 U, intramuscular) and were housed individually in cages. The rats were allowed to recover for 2 weeks.

Data acquisition

SEPs were recorded simultaneously over the 12 channels through a light-weight cable connected to a digital preamplifier. Data were recorded using an EEG/ERP system (CogniTrace ERP, ANT Inc., The Netherlands) and sampled at a rate of 2048 Hz together with the stimulus markers.

Experimental procedures

SEPs were evoked by applying brief electrical stimuli (2 ms duration, 6 mA), delivered by a DS7A constant

current stimulator (Digitimer Ltd, UK) to the volar surface of the left hind paw. To avoid habituation effects, low-intensity (0.5 mA) electrical stimuli were inserted randomly. Sixty stimuli (30 high-intensity and 30 low-intensity stimuli) were applied in a session. The interval between two sessions was fixed to 10 min. After injecting 5 mg/kg of morphine or saline (intraperitoneal), another two sessions were delivered. The interstimulus interval was 3500–5500 ms.

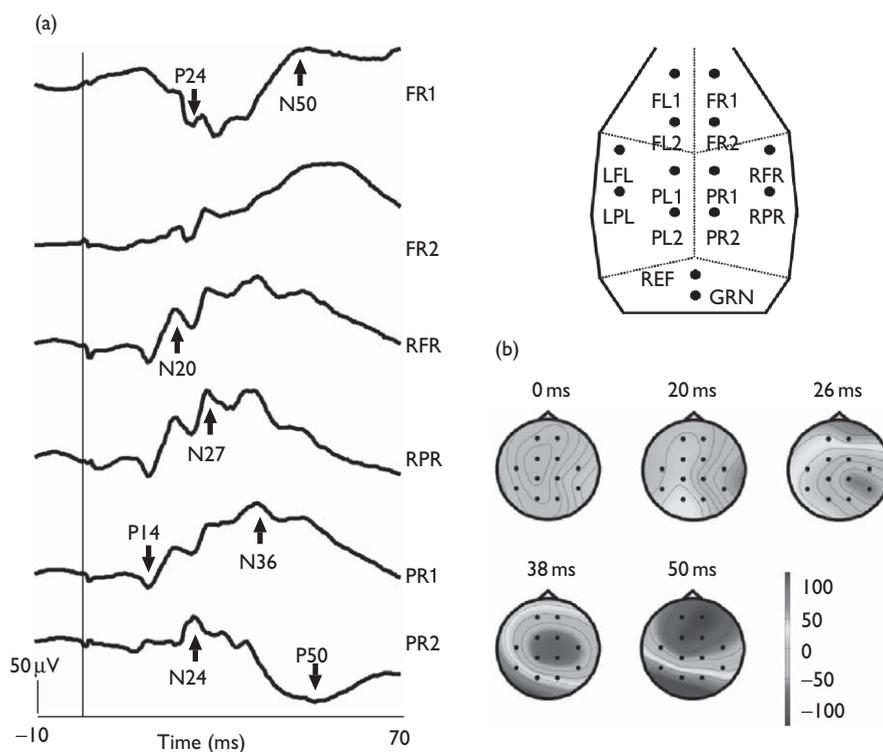
Measurement of pain threshold

Tail flick latency (TFL) in response to a radiant thermal stimulus was assessed with a 12.5 W projector bulb, according to the method of D'Amour and Smith [14]. The temperature was adjusted to obtain a baseline of 4–5 s. The cut-off time was set at 15 s. Before recording, the baseline pain threshold was measured by three tests with an interval of 5 min. Fifteen minutes after morphine or saline injection, TFLs were measured again every 5 min.

Data processing

Data epoch of 80 ms duration (10 ms prestimulus and 70 ms poststimulus) was analyzed offline using the EEGLAB software [15]. For separation and isolation of

Fig. 1



(a) Wide-band somatosensory-evoked potentials ($n=12$) after high-intensity electrical stimulation applied to the left hind paw of a rat. Arrows pointed to the components of the primary cortical response. (b) Grand mean topographies at different timepoints poststimulus. Note that the negative current activity shifted from the contralateral temporal region (20 ms) to primary somatosensory cortex area (26 ms), then to central area (38 ms) and finally located in frontal region (50 ms). Inset shows distribution of the 12 electrodes over the skull. FL, frontal left; FR, frontal right; LFL, left to frontal left; LPL, left to parietal left; PL, parietal left; PR, parietal right; RFR, right to frontal right; RPR, right to parietal right; GRN, ground.

the HFOs from original SEPs, the wide-band (10–2000 Hz) recorded responses were digitally filtered through a bandpass of 300–800 Hz. Independent component analysis was used to remove possible artifact. The character of HFOs and original SEPs were evaluated on the basis of responses recorded at channel RFR. The responses that exceeded the background noise level by 3 standard deviations were considered as signals. The noise level was measured between 5 and 10 ms after stimulus. The number of negative peaks, the interpeak latencies, amplitudes, durations, as well as the maximal amplitudes of HFOs were measured. The interpeak latencies of HFOs were averaged with values measured from two successive negative peaks. The amplitudes of HFOs were averaged with values measured from the vertical distance from a preceding positive peak to the following negative peak. The maximal amplitudes of HFOs were averaged from the real values of the negative peaks with the maximal amplitudes (the vertical distance from the

baseline to the maximal negative peaks). The duration of HFOs were measured from the onset to the offset of HFOs.

Differences in these parameters before and after morphine and saline injection were statistically analyzed using the Student's *t*-test. A value of *P* less than 0.05 was considered to be significant.

Results

Behavioral nociceptive responses

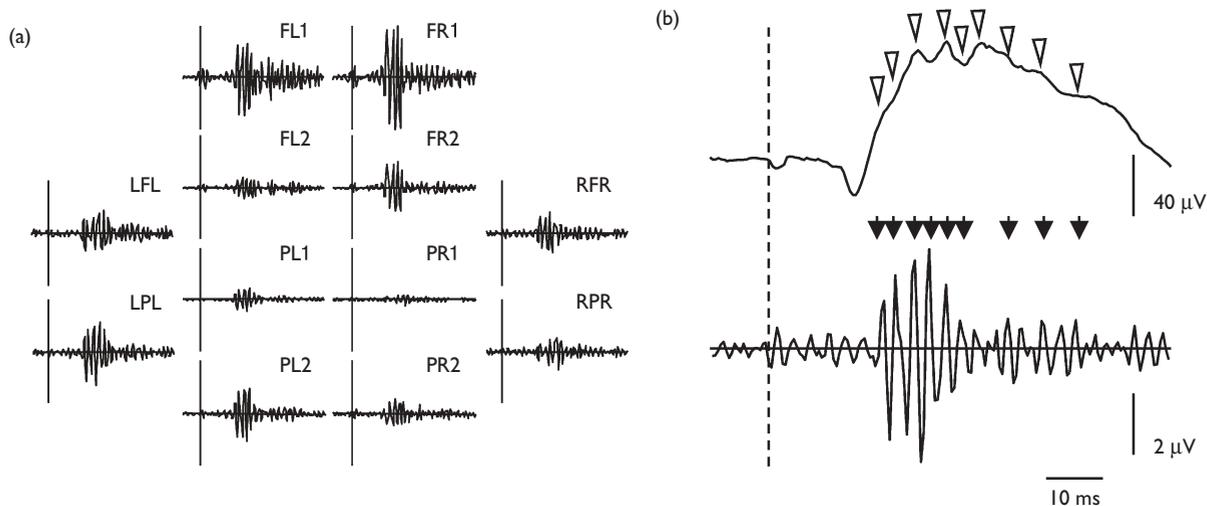
All rats showed obviously nociceptive behaviors after high-intensity electrical stimuli, including immediate withdrawal of the stimulated hind paw followed by aversive behavior, such as licking accompanied occasionally by gentle biting. The TFL was prolonged obviously by morphine injection (5.20 ± 1.47 vs. 14.80 ± 1.00 s, $P < 0.001$), whereas it remained unaffected after saline injection (4.68 ± 0.98 vs. 4.46 ± 1.16 s, $P > 0.05$).

Table 1 Comparison of wide-band somatosensory-evoked potentials before and after morphine or saline treatment

Peak	Latency (ms)				Amplitude (μV)			
	Pre-NS	Post-NS	Pre-Mor	Post-Mor	Pre-NS	Post-NS	Pre-Mor	Post-Mor
P14	14.43 ± 1.15	14.27 ± 1.36	14.27 ± 1.33	14.49 ± 1.36	22.45 ± 8.22	22.65 ± 7.9	19.08 ± 7.78	22.99 ± 10.25
N20	20.71 ± 1.52	20.35 ± 1.15	20.47 ± 1.11	20.22 ± 1.03	-50.72 ± 36.37	-55.1 ± 28.01	-51.47 ± 25.5	-61.92 ± 39.24
P24	24.74 ± 2.2	24.45 ± 1.05	24.95 ± 1.98	24.41 ± 2.19	57.86 ± 25.26	67.11 ± 35.54	62.19 ± 33.17	45.83 ± 15.17
N24	24.85 ± 0.79	24.41 ± 0.73	24.74 ± 0.65	24.07 ± 1.34	-37.89 ± 14.54	-43.42 ± 19.73	-39.26 ± 12.49	-40.77 ± 17.18
N27	27.17 ± 1.86	26.68 ± 1.68	27.17 ± 2.23	26.28 ± 3.73	-75.68 ± 33.84	-75.94 ± 24.34	-66.40 ± 18.85	-60.99 ± 21.55
N36	36.09 ± 2.92	38.85 ± 3.24	35.73 ± 2.25	34.46 ± 2.24	-98.81 ± 33.66	-97.49 ± 29.56	-84.12 ± 23.02	-93.32 ± 23.17
N50	50.03 ± 5.86	49.76 ± 6.01	48.03 ± 3.66	46.48 ± 3.07	-138.60 ± 64.22	-165.45 ± 73.31	-136.19 ± 47.41	-150.27 ± 55.29
P50	51.52 ± 3.98	52.16 ± 4.08	51.62 ± 6.05	49.54 ± 4.13	82.67 ± 28.53	80.75 ± 24.82	78.22 ± 25.83	91.82 ± 27.83

Post-Mor, after morphine treatment; Post-NS, after saline treatment; Pre-Mor, before morphine treatment; Pre-NS, before saline treatment.

Fig. 2



(a) An example of the high-pass-filtered (300–800 Hz) somatosensory-evoked potentials (SEPs) in 12 channels. High-frequency oscillation signals were extracted from traces in frontal and bilateral temporal regions. (b) The wide-band (10–2000 Hz) and high-pass-filtered (300–800 Hz) SEPs at channel RFR in a rat. Some little notches were observed on the ascending and descending slopes of the primary wide-band negative-evoked potential (upper trace). These little notches are corresponding to the high-frequency bursts in time domain (lower trace). The high-frequency bursts mainly superimposed on the ascending slope of the primary negative response. FL, frontal left; FR, frontal right; LFL, left to frontal left; LPL, left to parietal left; PL, parietal left; PR, parietal right; RFR, right to frontal right; RPR, right to parietal right.

Wide-band somatosensory-evoked potentials

In all rats, primary SEP components P14, N20, N/P24, N27, N36, and N/P50 could be clearly identified in traces contralateral to the stimulated side (Fig. 1a). The average latencies and amplitudes of each component in the four experimental conditions (before and after either saline or morphine injection) are shown in Table 1.

Topographies of SEPs after stimulation are shown in Fig. 1b. At 26 ms poststimulus, a negative activity over the contralateral primary somatosensory cortex was observed, which then shifted to midline (38 ms) and then to the frontal region (50 ms), where it reached the maximal amplitude.

The latencies and amplitudes of all these SEP components before and after morphine or saline treatment are shown in Table 1. There were no significant changes before and after either morphine or saline injection.

High-frequency somatosensory-evoked potentials

High-frequency oscillatory wavelets (300–800 Hz) that superimposed on the conventional SEPs evoked by high-intensity stimulation were detected at channels over parietal and frontal regions bilaterally (Fig. 2a). In the ascending and descending slopes of the primary negative wave, several little notches were detected (Fig. 2b). These little notches temporarily corresponded to the high-frequency bursts. Parameters of HFOs at channel RFR are listed in Table 2. High-frequency bursts mainly superimposed on the ascending slope of the primary negative wave. The number of HFO bursts from the onset to the peak of the primary negative is larger than that from the peak to the endpoint (Table 2).

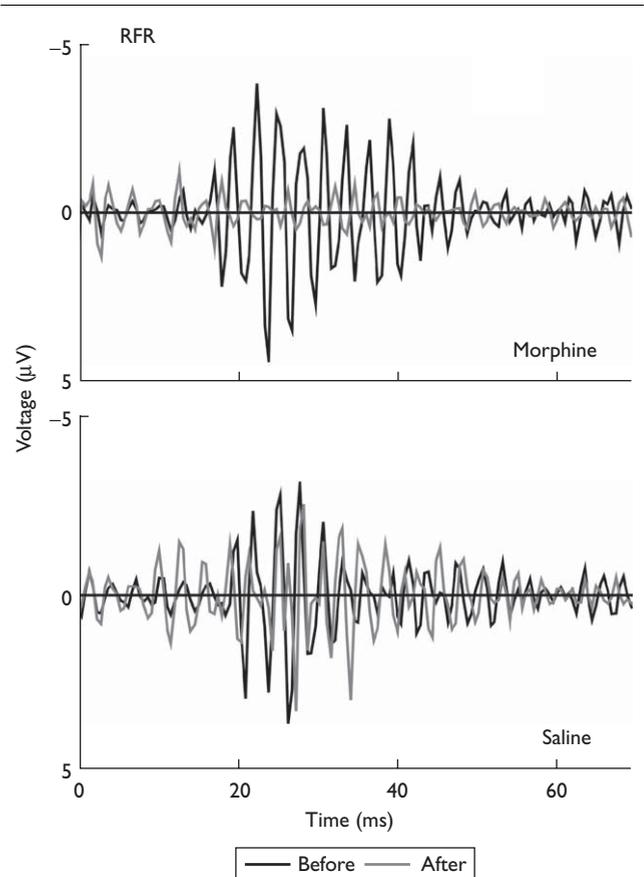
Systemic morphine showed a significant inhibitory effect on HFOs (Fig. 3, upper panel). The number of negative peaks, average amplitude, amplitude of the maximal negative peak, and HFO duration decreased significantly after morphine administration, whereas they remained unchanged by saline injection (Fig. 3, lower panel; Table 2).

Discussion

Cumulating evidence suggested that HFOs and conventional SEPs have different origins in the brain [6–8,11,16].

In human studies, the N20 response is known to be generated in Brodmann area 3b [5]. However, the origin of HFOs is still in dispute. Thalamus [17] and subthalamic sites [16] have been reported as possible sources of HFOs. Gobbelé *et al.* [9] suggested that HFOs reflected, at least in part, a burst of repetitive activity

Fig. 3



Comparison of high-frequency oscillations (HFOs) before and after morphine or saline treatment. The amplitude of HFOs after morphine injection (gray line, upper panel) was significantly smaller than that before morphine injection (black line, upper panel), while the amplitude of HFOs after saline (gray line, lower panel) did not differ significantly from that before saline injection (black line, lower panel).

Table 2 Comparison of HFOs before and after morphine or saline injection

	Morphine		Saline	
	Before	After	Before	After
Number of HFO negative peaks (total)	10.58 ± 2.68	5.75 ± 3.36**	8.67 ± 2.27	8.25 ± 4.43
Number of HFO negative peaks (onset–peak)	7.92 ± 4.83	4.83 ± 3.16*	7.33 ± 2.15	6.67 ± 3.11
Number of HFO negative peaks (peak–endpoint)	2.67 ± 1.72	0.92 ± 1.16***	1.33 ± 1.5	1.58 ± 2.11
HFO interpeak latency (ms)	2.49 ± 0.54	2.51 ± 0.49	2.41 ± 0.5	2.52 ± 0.55
HFO amplitude (total) (µV)	4.54 ± 1.97	3.19 ± 1.43***	4.59 ± 2.76	5.44 ± 3.09
Maximum amplitude of HFO (µV)	3.53 ± 1.38	2.37 ± 1.22**	3.97 ± 1.89	4.75 ± 2.33
HFO duration (ms)	29.67 ± 6.64	15.76 ± 12.37**	24.77 ± 7.12	24.01 ± 11.53

HFOs, high-frequency oscillations.

**P* < 0.05.

***P* < 0.01.

****P* < 0.001 vs. before.

conducted in the terminal segments of thalamocortical projection fibers initiated by the thalamic burst generator. A magnetoencephalographic study in pig detected highly synchronized repetitive spikes in thalamocortical axonal terminals and in postsynaptic intracortical cell populations [18]. In this study, electrical stimulation-evoked cerebral response distributed in the contralateral parietal area was observed at 26 ms post-stimulus, which is similar to that found in human studies. When filtering the raw data with a high-frequency bandpass, a set of HFO wavelets was detected. We also found that systemic morphine has no effect on conventional SEP components but significantly decreased the number and amplitude of HFOs. It is well known that high-intensity electrical stimulation can activate A δ nociceptor as well as A β mechanoreceptor. Cortical field potentials evoked by the activation of A δ nociceptor and A β mechanoreceptor cannot be affected by systemic morphine [19]. Our finding that systemic morphine has no effect on the primary SEP components agrees with previous finding. It has been proposed that supraspinal effects of morphine are primarily mediated at the thalamic level. A previous study showed that systemic morphine selectively depressed the nociceptive activity of thalamic neurons evoked either by thermal or by supramaximal percutaneous electrical stimuli [20]. The effect of morphine on HFOs observed in this study may result from the inhibitory effect of morphine on thalamus. Our results that morphine significantly decreased the number and amplitude of HFOs although having no effect on the amplitude and latency of primary SEP components provide additional evidence for their different origins.

In contrast to previous studies, we found that high-intensity electrical stimulation evoked high-frequency bursts widely distributed at the bilateral frontal and parietal lobes. The widespread distribution of HFOs found in this study may be because of the fact that the stimulus intensity applied in previous studies was greatly smaller than that used in this study.

The different behaviors of HFOs and conventional SEPs after morphine treatment indicate that they have different physiological functions. Halboni *et al.* [8] proposed that the high-frequency thalamic or cortical activity reflects a somatosensory arousal system. In this study, the randomly inserted low-intensity stimulation evoked only low-amplitude HFOs in the parietal channels (data not shown), whereas widely distributed HFOs with high amplitude were evoked after high-intensity electrical stimulation. The amplitude of HFOs evoked by high-intensity stimulation was reduced dramatically by systemic morphine. The higher amplitude and wide distribution of HFOs after high-intensity stimulation and the dramatic reduction of HFOs after morphine both suggested the vigilance-dependent property of HFO.

We speculate that conventional early SEPs reflect the location of stimulus, whereas HFOs reflect the cortical arousal elicited by stimulation.

Conclusion

In conclusion, dissociated behaviors of HFOs and conventional SEPs after systemic morphine administration were observed in this study, indicating different origins. These findings implicate that HFOs and conventional SEPs are functionally different in sensory processing.

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